

Contents lists available at ScienceDirect

Journal of the Neurological Sciences

journal homepage: www.elsevier.com/locate/jns

An incomplete Circle of Willis is not a risk factor for white matter hyperintensities: The Tromsø Study

Lars B. Hindenes^{a,b,*}, Asta K. Håberg^{c,d}, Ellisiv B. Mathiesen^{a,e}, Torgil R. Vangberg^{a,b}^a Department of Clinical Medicine, Faculty of Health Sciences, UiT The Arctic University of Norway, Postboks 6050 Langnes, 9037 Tromsø, Norway^b PET Centre, University Hospital of North Norway, 9038 Tromsø, Norway^c Department of Radiology and Nuclear Medicine, St. Olav University Hospital, Postboks 3250 Torgarden, 7030 Trondheim, Norway^d Department of Neuromedicine and Movement Science, Norwegian University of Science and Technology (NTNU), NTNU 7491 Trondheim, Norway^e Department of Neurology, University Hospital of North Norway, 9038 Tromsø, Norway

ARTICLE INFO

Keywords:

Circulation

Leukoaraiosis

Health survey

Epidemiology

ABSTRACT

Objective: The Circle of Willis (CoW) is often underdeveloped or incomplete, leading to suboptimal blood supply to the brain. As hypoperfusion is thought to play a role in the aetiology of white matter hyperintensities (WMH), the objective of this study was to assess whether incomplete CoW variants were associated with increased WMH volumes compared to the complete CoW.

Methods: In a cross-sectional population sample of 1751 people (age 40–84 years, 46.4% men), we used an automated method to segment WMH using T1-weighted and T2-weighted fluid-attenuated inversion recovery image obtained at 3T. CoW variants were classified from time-of-flight scans, also at 3T. WMH risk factors, including age, sex, smoking and blood pressure, were obtained from questionnaires and clinical examinations. We used linear regression to examine whether people with incomplete CoW variants had greater volumes of deep WMH (DWMH) and periventricular WMH (PWMH) compared to people with the complete CoW, correcting for WMH risk factors.

Results: Participants with incomplete CoW variants did not have significantly higher DWMH or PWMH volumes than those with complete CoW when accounting for risk factors. Age, pack-years smoking, and systolic blood pressure were risk factors for increased DWMH and PWMH volume. Diabetes was a unique risk factor for increased PWMH volume.

Conclusion: Incomplete CoW variants do not appear to be risk factors for WMH in the general population.

1. Introduction

White matter hyperintensities (WMH) are seen as a marker of cerebral small vessel disease [51]. They are common in older adults, and their prevalence rapidly increases with age [5]. WMH have been associated with cognitive decline and dementia [6], and impaired motor function [15]. Risk factors of cerebrovascular disease have also been associated with WMH, including hypertension [10,46,47], type 1 and 2 diabetes [20,25], body mass index (BMI) [25], and smoking [16,20,47].

Although the aetiology of WMH is not fully understood [51], hypoperfusion may play a role as histology shows signs of hypoxia in WMH [12] and WMH commonly occur in watershed regions in cerebral white matter.

The Circle of Willis (CoW), located at the base of the brain, is an anastomosis of the carotid arteries and the basilar artery. Its circular structure enables redistribution of the cerebral blood flow in case of reduced upstream flow, subsequently providing redundancy to the brain's blood supply. However, it is very common that at least one of the

Abbreviations: CoW, Circle of Willis; WMH, white matter hyperintensities; DWMH, deep white matter hyperintensities; PWMH, periventricular white matter hyperintensities; MPRAGE, magnetisation prepared rapid acquisition gradient-echo; GRAPPA, Generalized Autocalibrating Partially Parallel Acquisition; FLASH, fast low angle shot; TOF, time-of-flight; FLAIR, fluid-attenuated inversion recovery; T1w, T1-weighted; SVD, small vessel disease; MNI, Montreal Neurological Institute; ANTs, Advanced Normalization Tools.

* Corresponding author at: Department of Clinical Medicine, Faculty of Health Sciences, UiT The Arctic University of Norway, Postboks 6050 Langnes, 9037 Tromsø, Norway.

E-mail addresses: lars.b.hindenes@uit.no (L.B. Hindenes), asta.haberg@ntnu.no (A.K. Håberg), ellisiv.mathiesen@uit.no (E.B. Mathiesen), torgil.vangberg@uit.no (T.R. Vangberg).

<https://doi.org/10.1016/j.jns.2020.117268>

Received 7 October 2020; Received in revised form 18 November 2020; Accepted 9 December 2020

Available online 13 December 2020

0022-510X/© 2020 The Author(s). Published by Elsevier B.V. This is an open access article under the CC BY license (<http://creativecommons.org/licenses/by/4.0/>).

segments in the CoW are hypoplastic or missing. A recent dissection study found that only 7% of adults have a complete CoW [52], suggesting that the CoW does not inherently have a critical influence on human survival. A non-patent CoW may, however, cause suboptimal blood supply to some brain regions due to diminished collateral capacity, particularly in combination with atherosclerosis or other arterial occlusions.

Indeed, previous studies have found an association between incomplete CoW variants and increased WMH burden. In a convenience sample of 163 patients, it was found that patients with incomplete variants had a significantly higher Fazekas score compared to those with a complete CoW [37]. In patients with carotid artery stenosis, incomplete CoW variants were associated with greater WMH volume and number of WMH lesions [38,39], increased WMH rating [4], and increased deep WMH (DWMH) and periventricular WMH (PWMH) ratings [54]. However, the results are not unison, as some studies fail to find a link between more WMH and decreased completeness of the CoW, both in patients with carotid stenosis [29,45] and in the general population [7]. Interestingly, atherosclerosis patients with an incomplete CoW also have more carotid intraplaque haemorrhage than those with a complete CoW [56]. As carotid intraplaque haemorrhage accelerate plaque progression [42] this may pose an additional risk for WMH in people with incomplete CoW, and indeed carotid intraplaque haemorrhage has been associated with increased WMH volume [1]. Despite diverging results from prior studies, there is evidence suggesting that an incomplete CoW may be a risk factor for WMH possibly via impaired autoregulation of cerebral blood flow [19] which has been shown to be associated with WMH [33]. Furthermore, PWMH is more strongly associated with cerebral blood flow [43], blood pressure [17] and vasculature in general [2] than DWMH. Therefore, PWMH may be more sensitive to variations in the CoW than DWMH, and this may in part explain possible diverging findings relating to WMH and anatomical variants of the CoW. Since WMH and also incomplete CoW variants [11,21,55] are more prevalent among older people, it is of interest to examine whether incomplete CoW variants pose a risk of WMH in the general population.

In this study, we therefore assessed whether incomplete CoW variants might be risk factors for increased WMH burden in a large population-based sample of middle-aged and older people. We grouped the incomplete CoW variants according to the segments of the CoW that were missing, similar to Saba et al. [39], as opposed to broad categories (e.g. incomplete/complete CoW), since this would increase the sensitivity of detecting specific CoW variants strongly associated with WMH. We used linear regression models to compare DWMH and PWMH volumes of each incomplete CoW variant to the complete variant while correcting for cerebrovascular risk factors.

2. Methods

The study was approved by the Regional Committee of Medical and Health Research Ethics Northern Norway (2014/1665/REK-Nord) and carried out in accordance with relevant guidelines and regulations at UiT The Arctic University of Norway. All participants gave written informed consent before participating in the study.

2.1. Study population

Eligible for the study were 1864 participants (40–84 years) of the seventh wave of the population-based Tromsø Study [30] who underwent time-of-flight (TOF) MRI scanning of the brain and had complete imaging data [21]. We excluded participants with image artefacts or brain pathology that could lead to unreliable WMH volume estimates, and participants with rare CoW variants (less than ten observations) as parameter estimates would be unreliable.

2.2. MRI protocol

Participants were scanned at the University Hospital North Norway with the same 3T Siemens Skyra MR scanner (Siemens Healthcare, Erlangen, Germany). We used a 64-channel head coil in the majority of examinations, but in 38 examinations a slightly larger 20-channel head coil had to be used to accommodate the participants' head. The MRI protocol consisted of T1-weighted (T1w), T2-weighted fluid-attenuated inversion recovery (FLAIR), TOF angiography and susceptibility-weighted sequences.

T1w images were acquired with a 3D magnetisation prepared rapid acquisition gradient-echo (MPRAGE) sequence (flip angle = 9°, TR/TE/TI = 2300 ms/4.21 ms/996 ms). The T2-weighted FLAIR images were acquired with a 3D turbo spin-echo sequence with variable flip angle (TR/TE/TI = 5000 ms/388 ms/1800 ms, partial Fourier = 7/8). The T1w and FLAIR scans were acquired sagittally with 1 mm isotropic resolution, Generalized Autocalibrating Partially Parallel Acquisition (GRAPPA) parallel imaging acceleration factor 2, FOV = 256 mm, 176 slices, 1 mm slice thickness, and 256 × 256 image matrix. The T1w and FLAIR were used to measure the WMH volume. TOF angiography images were acquired with a 3D transversal fast low angle shot (FLASH) sequence with flow compensation (TR/TE = 21/3.43 ms, GRAPPA parallel imaging acceleration factor 3, FOV 200 × 181 mm, slice thickness 0.5 mm, 7 slabs with 40 slices each). Reconstructed image resolution was 0.3 × 0.3 × 0.5 mm.

2.3. Defining Circle of Willis segments and mirrored variants

The CoW consists of the left and right proximal anterior cerebral artery (A), the anterior communicating artery (Ac), the left and right posterior communicating artery (Pc), and the left and right proximal posterior cerebral artery (P). In figures and tables, we refer to the complete CoW variant as "O", while the incomplete variants are denoted by their missing segments. We also did not differentiate between left-right mirrored CoW variants in order to reduce the number of tested variants. Including the complete variant, we then had in total 17 unique CoW variants to be included in statistical testing (Fig. 1). The classification of anatomical variants in the CoW was done in a previous study, in which segments not visible or with a diameter less than 1 mm were classified as missing/hypoplastic [21]. The previous study identified 47 unique CoW variants [21], but due to exclusion of some participants and merging of left-right symmetrical CoW variants, we ended up with 17 variants. Specifically, we first excluded participants with no WMH measurement such that 45 unique CoW variants remained. Then, due to merging of 30 left-right mirrored CoW variants 30 unique CoW variants remained. At last, due to removing CoW variants having less than ten observations the 17 unique CoW variants remained.

2.4. WMH segmentation

We segmented WMH using a fully convolutional neural network algorithm [28] using the T1w and FLAIR images as input. The algorithm used 2D convolution in a U-NET architecture with different data pathways to evaluate images slice by slice. Despite not using 3D convolution, this algorithm was the best performer in the WMH Segmentation Challenge at MICCAI 2017 [27] and was trained on images from five different scanners. The algorithm should therefore be more robust for use on images from a different scanner, compared to an algorithm that is trained on images from only one scanner.

The T1w and FLAIR images were first co-registered, and then rigid body aligned to the MNI (i.e. Montreal Neurological Institute) template using ANTs (i.e. Advanced Normalization Tools) toolkit (<http://stnava.github.io/ANTs/>, v.2.3.1). The latter was done to ensure consistent orientation of the images, which were found to improve the reliability of the U-NET algorithm. We ran the U-NET algorithm following Li's and colleagues' recommendations [28] and with default settings, except that

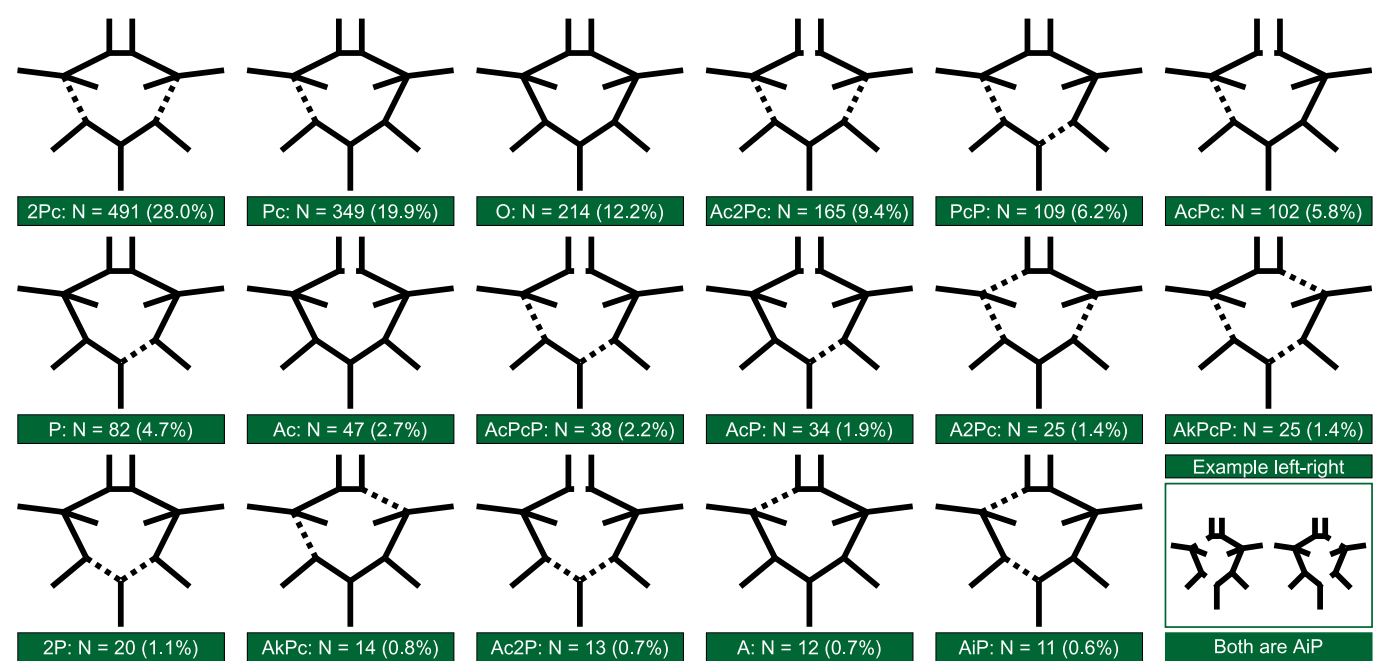


Fig. 1. The 17 Circle of Willis variants used in the analyses. “N” and “%” denotes count and percentage of each variant. If asymmetric, each schematic Circle of Willis and label contain both left and right variants as shown by the example in the lower right corner. “i” = ipsilateral and “k” = contralateral relationship between two subsequent segments. Prefix “2” denotes that both left and right segments are missing. “A” = proximal anterior cerebral artery, “Ac” = anterior communicating artery, “Pc” = posterior communicating artery, “P” = proximal posterior cerebral artery, and “O” = complete Circle of Willis.

we did not use bias-field correction, as an initial validation showed that this degraded the segmentation. After U-NET, the segmentation was corrected for misclassifications in grey matter by applying a white matter mask derived from the FreeSurfer (v6.0) subcortical

segmentation of the T1w images [13,14]. We validated the WMH segmentation against 30 manually segmented images with a wide range of WMH volumes, from almost no WMH to severe volumes. A master student in the field of medicine

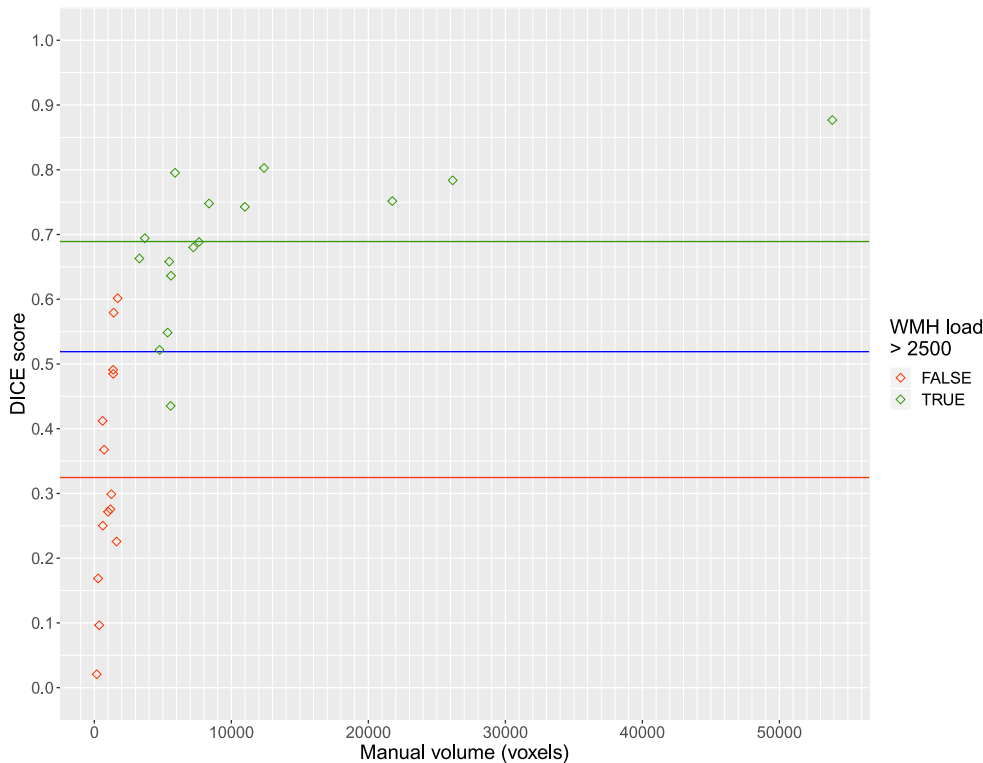


Fig. 2. Validation of the WMH segmentation algorithm: Dice score and relative absolute volume difference between ground truth WMH and segmented WMH. The blue line shows the overall mean Dice score, while the green and red line show the mean Dice score for segmentations with respective ground truth WMH load over and under 2500 voxels. (For interpretation of the references to colour in this figure legend, the reader is referred to the web version of this article.)

manually segmented the WMH with supervision from author TRV. The automatic segmentation showed similar performance in terms of the similarity coefficient Dice (mean Dice = 0.519 [SD = 0.234]) compared to many other available WMH segmentation methods [18,23,24,35,41,44]. Note that the Dice score becomes more sensitive to errors at small volumes, thereby decreasing the mean Dice score for the validation dataset, but for participants with WMH volumes >2.5 ml (2500 voxels) the individual Dice scores were almost always greater than the overall mean Dice score, averaging close to 0.7, see Fig. 2.

2.5. Partitioning WMH into deep and periventricular segments

We partitioned the WMH masks into PWMH and DWMH using a 10 mm distance from the ventricles. We chose 10 mm as a threshold based on a recent study [17] which showed that this threshold gives the most comparable results to previous studies and also the best separation between PWMH and DWMH in terms of the cardiovascular risk factors. Masks separating PWMH and DWMH were created by spherically dilating ventricle masks from the FreeSurfer segmentation by 10 mm.

2.6. Demographic and WMH risk variables

We included ten adjustment variables in our models that have been associated with WMH: age [31,47], sex [31,36], BMI [25], education [20], smoking [16,20,47] as pack-years, diabetes [20,25], blood glucose levels [3], high-sensitive C-reactive protein (CRP) levels [40], systolic blood pressure (SBP) [10,46,47], and total cholesterol to high-density lipoprotein (HDL) ratio [9]. The independent and dependent variables are further characterised in Table 1. Missing values in continuous variables were imputed by mean or median depending on their distribution, and missing values in categorical variables were imputed by rounded median.

2.7. Statistical analysis

All statistical analyses were done with R (v3.5.2). In the linear regression analyses, we used (1) DWMH volume, and (2) PWMH volume as dependent variables. Both volume estimates were log-transformed to better satisfy normality and homoscedasticity assumptions, and we added 1 voxel (1 cubic mm) to all volumes before the log transformation to avoid log of zero. For each dependent variable, we fitted a model including age, sex, CoW variants, and risk factors; i.e. each model has ten risk factors, and 17 factors for each of the incomplete CoW variants including the complete CoW used as a common reference. The beta coefficients presented for these variables were not adjusted.

Post-hoc multiple comparisons of means with Dunnett contrasts were used to test whether the incomplete CoW variants had higher WMH volumes compared to the complete CoW variant (i.e. a one-sided test). This was done separately for each model. Each post-hoc comparison reports step-down Dunnett adjusted *p*-values relative to the conventional significance level for one-sided comparisons. The R package “multcomp” [22] was used to calculate the post-hoc comparisons with adjusted *p*-values based on the linear regression models. The corresponding confidence intervals constructed to calculate *p*-values were stochastic, making exact replication without a seed unlikely. To avoid an unwarranted increase in the probability of committing type 1 errors, at the cost of slightly increased risk of type 2 error, we corrected only for multiple tests within linear regression models as described, but not between models. We regarded the conventional $p < 0.05$ as significant.

3. Results

3.1. Study participants

Of the 1864 participants, 76 were excluded due to atrophy or image artefacts that might have led to inaccurate WMH volume estimates, then

Table 1

Characteristics of the study participants.

Variable	Unit or Factor	Measurement	Missing*	Min	Max
Age	Year	63.51 (10.63)	0	40.00	84.00
Sex	Female	938 (53.6)	0		
	Male	813 (46.4)			
Education	Up to 10 years	509 (29.7)	37		
	High school: 3+ years	471 (27.5)			
	Up to 4 years at university	340 (19.8)			
	More than 4 years at university	394 (23.0)			
	mmHg				
SBP		133.96 (20.79)	6	78.00	220.00
Hypertension [#]	No	1070 (61.3)	6		
	Yes	675 (38.7)			
Cholesterol to HDL ratio		3.67 (1.35)	7	1.28	23.00
CRP, median [IQR]	mg/L	1.02 [0.59, 2.08]	7	0.14	58.98
Smoke daily	Yes, now	222 (12.8)	18		
	Yes, previously	839 (48.4)			
	Never	672 (38.8)			
Pack years		9.39 (12.87)	71	0.00	90.00
BMI		27.15 (4.20)	1	13.90	45.90
Diabetes ⁺	No	1587 (93.6)	55		
	Yes	109 (6.4)			
Glucose	mmol/L	5.74 (1.65)	3	2.70	19.20
Total WMH, median [95% CI]	mm ³	2113 [505, 31584]	0	0	110447
DWMH, median [95% CI]	mm ³	699 [221, 9734]	0	0	41634
PWMH, median [95% CI]	mm ³	1332 [166, 21725]	0	0	74558

Unless specified, continuous variables are given as mean (standard deviation), and categorical variables as count (percentage). Abbreviations: WMH = white matter hyperintensities, DWMH = deep white matter hyperintensities, PWMH = periventricular white matter hyperintensities, CRP = C-reactive protein, SBP = systolic blood pressure, MMS = mini mental status, BMI = body mass index, HDL = high density lipoprotein, CI = credible interval, IQR = interquartile range, and SD = standard deviation. * Missing values were imputed before analysis. [#] Hypertension were defined as systolic blood pressure ≥ 140 mmHg or diastolic blood pressure ≥ 90 mmHg. ⁺ Diabetes category includes both type 1 and type 2.

11 were excluded due to failures in the segmentation algorithm, and at last 26 were excluded due to having a rare CoW variant (see Fig. 3). For the 1751 participants included in our analyses, mean age was 63.5 years (SD = 10.6). Men were on average 64.3 years (SD = 10.5), and women 62.8 years (SD = 10.7). Further sample characteristics of the 1751 participants are shown in Table 1.

3.2. Deep WMH model with post-hoc multiple comparisons

There was no incomplete CoW variant with significantly higher DWMH volume compared to the complete CoW variant in the post-hoc multiple comparisons. The PcP variants were the only CoW with an adjusted *p*-value under 50% ($t = 2.457$, adjusted $p = 0.093$) and its unadjusted equivalent two-sided *p*-level was significant at 0.05 (Table 2). Altogether this suggests that the PcP variants trended to have more DWMH than the complete variant. The R^2 for the regression model was 0.167, indicating that this model did not explain DWMH well.

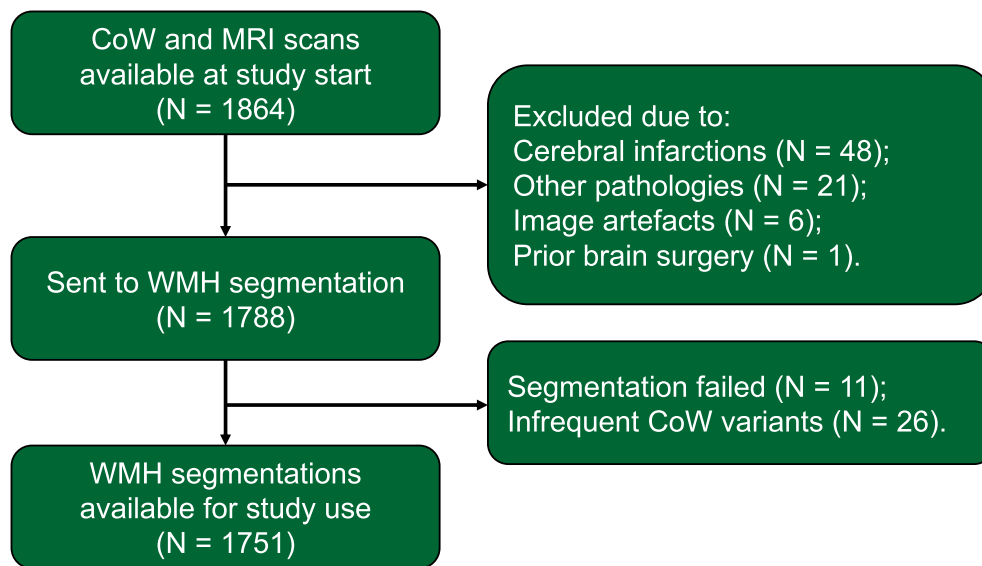


Fig. 3. Flow diagram of the sample selection process. “CoW” = Circle of Willis, “WMH” = White matter hyperintensities.

Table 2

Regression model coefficients for DWMH and PWMH. p-levels denoted by asterisk in the table are from unadjusted two-sided tests in the models included for gauging risk of type 1 error, and not results of the one-sided post-hoc analysis.

	DWMH	PWMH
Intercept	4.2089 ***	1.5267 ***
2P	0.2239	0.1304
2Pc	0.0787	−0.0072
A	0.0120	−0.0038
A2Pc	−0.2962	−0.5055 *
Ac	0.1138	−0.0132
Ac2P	0.1511	−0.0213
Ac2Pc	0.0629	−0.0585
AcP	−0.0431	−0.1081
AcPc	0.1591	−0.0477
AcPcP	−0.1860	−0.2458
AiP	−0.3697	−0.6014
AkPc	−0.1531	−0.3895
AkPcP	−0.1151	−0.2869
P	−0.1346	−0.3931 **
Pc	−0.0078	−0.0829
PcP	0.2714 *	0.1120
Age	0.0301 ***	0.0789 ***
Sex male	−0.0584	0.0641
BMI	−0.0040	0.0045
Education 2	−0.0942	−0.0821
Education 3	−0.0465	−0.0396
Education 4	−0.0921	−0.0231
Cholesterol to HDL ratio	0.0104	−0.0073
Pack year	0.0048 **	0.0057 **
CRP	0.0028	0.0191
SBP	0.0041 ***	0.0041 **
Diabetes	0.1973	0.4280 ***
Glucose	0.0284	0.0196
R ²	0.1671	0.4582

*** $p < 0.001$; ** $p < 0.01$; * $p < 0.05$.

Abbreviations: WMH = white matter hyperintensities, CRP = C-reactive protein, SBP = systolic blood pressure, BMI = body mass index, and HDL = high density lipoprotein.

3.3. Periventricular WMH model with post-hoc multiple comparisons

For the PWMH model (Table 2), no incomplete CoW variants had significantly higher PWMH volume compared to the complete CoW variant in the post-hoc multiple comparisons analysis. All adjusted p -

values were between 0.85 and 1. In terms of the two-sided p -levels, the P and A2Pc variants had negative coefficients significant at 0.01 and 0.05, respectively, explaining why the one-sided post-hoc analysis was non-significant. The R^2 for the regression model was 0.458, and also considerably higher than for the DWMH model. This indicates that the same set of vascular risk factors and incomplete CoW variants in the regression models explained PWMH volume better than DWMH volume.

4. Discussion

In this population-based study, we examined whether participants with incomplete CoW variants had increased WMH volumes compared to those with the complete CoW. The main findings were that neither PWMH or DWMH volumes were significantly increased in participants with incomplete CoW variants relative to participants with a complete CoW when correcting for age, gender and WMH risk factors. To our knowledge, only one previous study has examined whether there is an association between the completeness of the CoW and WMH in the general population [7]. This study examined older participants from a native South American population, that have a high prevalence of small vessel disease (SVD), but failed to find any association between an incomplete CoW and increased WMH [7] and markers of SVD in general [8]. Our results, together with these findings suggest that anatomical variations in the CoW are not substantial risk factors for increased DWMH and PWMH volumes in the general population aged 40 years or older.

Our results differ from previous studies that have found an association between incomplete CoW variants and increased WMH load. Most of these studies are on patients with carotid artery stenosis [4,38,39,54]. For this patient group, there is a clear mechanism connecting the CoW anatomy and WMH, i.e., the stenosis will render the collateral capacity of the CoW important for maintaining sufficient blood flow to the brain. The association between the incompleteness of CoW and lower WMH load in atherosclerosis patients together with our negative results on generally healthy participants suggests that collateral flow in the CoW may only be protective against WMH when arteries upstream to the CoW are stenotic or occluded. However, it is difficult to firmly conclude that an incomplete CoW is a risk factor for WMH even in patients with carotid artery stenosis as some studies have failed to find such an association [29,45].

The inconsistent results on whether a complete CoW may be protective against WMH may hint of a more complex role of the CoW in the

cerebrovascular system than just having the role as a compensatory system in case of arterial occlusion. This has been suggested by previous studies [32,50]. In particular, Vrselja et al. argued that the CoW also plays a role in blood pressure dissipation, ensuring lower fluctuations in blood pressure in the downstream cerebral arteries of the CoW [50]. It is conceivable that hypoplastic segments with a diameter less than 1 mm may have an important role in dissipating fluctuations in blood pressure, but only a minor role in collateral blood flow. As greater pressure fluctuations in the blood flow are associated with WMH [33], the dampening of blood pressure fluctuations in the CoW may be just as crucial as its collateral ability. Unfortunately, we did not distinguish between missing and hypoplastic segments, similarly to most other TOF imaging studies on the CoW [7,11,26,34,39], since it is near impossible to distinguish between missing and hypoplastic segments reliably from TOF images.

As expected, some of the WMH risk factors were associated with increased DWMH and PWMH. Interestingly, diabetes was only associated with increased PWMH, lending support to the notion that DWMH and PWMH have differing aetiology [2,43]. Also, vascular risk factors, age and gender explained 45.8% of the variance in PWMH, while only 16.7% of the variance of DWMH, suggesting that PWMH is more closely associated with cerebrovascular disease than DWMH.

There are some limitations to our study warranting discussion. First, it is conceivable that other measurements of the CoW might offer greater insight into a potential connection between the CoW anatomy and WMH; e.g. considering the diameters of the arterial segments and, as already discussed, distinguishing between hypoplastic and absent segments. Second, we divided the WMH volume into deep and periventricular components which can make our study difficult to compare with other studies. Third, it is possible that partitioning the WMH volume in the individual flow territories would be more sensitivity to variations in the CoW anatomy. Still, we decided against this because flow territories depend on the CoW anatomy [48]. Fourth, we were unable to distinguish between diabetes type 1 and type 2, but most diabetes cases are generally of type 2 in a western population [53]. Fifth and last, most previous studies on the connection between WMH and CoW have grouped the anatomical variations of the CoW into broad categories (e.g. missing segments in the anterior or posterior circulation), instead of comparing unique variants as we have done. The rationale for this was that it might provide greater sensitivity, but it also complicates the comparison to previous studies.

The strengths of the study are the large cross-sectional population-based sample with reliable information on relevant risk factors. We also used a state of the art automatic WMH segmentation software to avoid WMH rater biases. Use of such automatic software has also increased the replicability of our study and allowed us to use WMH volumes instead of discrete scales, as this is found to offer greater sensitivity in correlations with clinical measures [49]. Our CoW classification also has acceptable intra and inter rater accuracy [21]. Furthermore, due to our large sample we, were able to include 17 unique CoW variants in the models without compromise in model assumptions. We applied the liberal step-down Dunnett correction for multiple tests, compared to Bonferroni, to reduce chance of type 2 errors. We also provided information about regressions' two-sided p-levels enabling some insight about chance of type 1 errors or whether our post hoc analysis had missed possible negative associations not originally hypothesized as relevant.

5. Conclusions

In this large population sample of people aged 40 and older, incomplete CoW variants are not substantial risk factors for increased DWMH and PWMH volumes.

Funding

This work was supported by two Helse Nord project grants

HNF1369-17 and SFP1271-16, and computational resources from NOTUR grant #NN9562K. The funding source had no role in the study design, collection of data, analysis, interpretation of data, and in the decision to submit the article for publication.

Data availability statement

Ethical and legal restrictions prohibit the authors from making the dataset available outside The Tromsø Study database, which is available by contacting The Tromsø Study. Please see https://en.uit.no/forskning/forskningsgrupper/sub?p_document_id=453582&sub_id=669706 for detail on how to obtain access to all relevant data.

Declaration of Competing Interest

None.

Acknowledgements

We thank the participants of the Tromsø Study, the administration of the Tromsø Study, the Department of Radiology at the University Hospital North Norway and the MR imaging technologists for their contributions to the study. Special thanks to Liv Hege Johnsen for helpful discussions and assistance with the data curation process.

References

- [1] N. Altaf, P.S. Morgan, A. Moody, S.T. MacSweeney, J.R. Gladman, D.P. Auer, Brain white matter hyperintensities are associated with carotid intraplaque hemorrhage, *Radiology* 248 (2008) 202–209, <https://doi.org/10.1148/radiol.2481070300>.
- [2] N.J. Armstrong, K.A. Mather, M. Sargurupremraj, M.J. Knol, R. Malik, C. L. Satizabal, L.R. Yanek, W. Wen, V.G. Gudnason, N.D. Dueker, L.T. Elliott, E. Hofer, J. Bis, N. Jahanshad, S. Li, M.A. Logue, M. Luciano, M. Scholz, A.V. Smith, S. Trompet, D. Vojinovic, R. Xia, F. Alfaro-Almagro, D. Ames, N. Amin, P. Amouyel, A.S. Beiser, H. Brodaty, I.J. Deary, C. Fennema-Notestine, P.G. Gampawar, R. Gottesman, L. Griffanti, C.R. Jack, M. Jenkinson, J. Jiang, B.G. Kral, J.B. Kwok, L. Lampe, C.M. Liewald, P. Maillard, J. Marchini, M.E. Bastin, B. Mazoyer, L. Pirpamer, J. Rafael Romero, G.V. Roshchupkin, P.R. Schofield, M.L. Schroeter, D.J. Stott, A. Thalamuthu, J. Trollor, C. Tzourio, J. van der Grond, M.W. Vernooij, V.A. Witte, M.J. Wright, Q. Yang, Z. Morris, S. Sigurdsson, B. Psaty, A. Villringer, H. Schmidt, A.K. Haberg, C.M. van Duijn, J.W. Jukema, M. Dichgans, R.L. Sacco, C. B. Wright, W.S. Kremen, L.C. Becker, P.M. Thompson, T.H. Mosley, J.M. Wardlaw, M.A. Ikram, H.H.H. Adams, S. Seshadri, P.S. Sachdev, S.M. Smith, L. Launer, W. Longstreth, C. DeCarli, R. Schmidt, M. Fornage, S. Debette, P.A. Nyquist, Common genetic variation indicates separate causes for periventricular and deep white matter hyperintensities, *Stroke* 51 (2020) 2111–2121, <https://doi.org/10.1161/STROKEAHA.119.027544>.
- [3] N. Cherbuin, W. Wen, P.S. Sachdev, K.J. Anstey, Fasting blood glucose levels are associated with white matter hyperintensities' burden in older individuals with and without type 2 diabetes, *J. Neurol. Sci.* 357 (2015), e44, <https://doi.org/10.1016/j.jns.2015.08.189>.
- [4] Y.-M. Chuang, K.-L. Huang, Y.-J. Chang, C.-H. Chang, T.-Y. Chang, T.-C. Wu, C.-P. Lin, H.-F. Wong, S.-J. Liu, T.-H. Lee, Associations between circle of Willis morphology and white matter lesion load in subjects with carotid artery stenosis, *Eur. Neurol.* 66 (2011) 136–144, <https://doi.org/10.1159/000329274>.
- [5] F.-E. de Leeuw, Prevalence of cerebral white matter lesions in elderly people: a population based magnetic resonance imaging study. The Rotterdam Scan Study, *J. Neurol. Neurosurg. Psychiatry* 70 (2001) 9–14, <https://doi.org/10.1136/jnnp.70.1.9>.
- [6] S. Debette, H.S. Markus, The clinical importance of white matter hyperintensities on brain magnetic resonance imaging: systematic review and meta-analysis, *BMJ* 341 (2010) c3666, <https://doi.org/10.1136/bmj.c3666>.
- [7] O.H. Del Brutto, J. Lama, Variants in the circle of Willis and white matter disease in ecuadorian mestizos, *J. Neuroimaging* 25 (2015) 124–126, <https://doi.org/10.1111/jon.12077>.
- [8] O.H. Del Brutto, R.M. Mera, M. Zambrano, J. Lama, Incompleteness of the circle of Willis correlates poorly with imaging evidence of small vessel disease. A population-based study in rural Ecuador (the Atahualpa project), *J. Stroke Cerebrovasc. Dis.* 24 (2015) 73–77, <https://doi.org/10.1016/j.jstrokecerebrovasdis.2014.07.036>.
- [9] D.A. Dickie, S.J. Ritchie, S.R. Cox, E. Sakka, N.A. Royle, B.S. Aribisala, Valdés Hernández, M.C. Del, S.M. Maniega, A. Pattie, J. Corley, J.M. Starr, M. E. Bastin, I.J. Deary, J.M. Wardlaw, Vascular risk factors and progression of white matter hyperintensities in the Lothian birth cohort 1936, *Neurobiol. Aging* 42 (2016) 116–123, <https://doi.org/10.1016/j.neurobiolaging.2016.03.011>.
- [10] C. Dufouil, A. de Kersaint-Gilly, V. Besancon, C. Levy, E. Auffray, L. Brunnerneau, A. Alperovitch, C. Tzourio, Longitudinal study of blood pressure and white matter

- hyperintensities: the EVA MRI cohort, *Neurology* 56 (2001) 921–926, <https://doi.org/10.1212/WNL.56.7.921>.
- [11] E. El-Barhoun, S. Gledhill, A. Pitman, Circle of Willis artery diameters on MR angiography: an Australian reference database, *J. Med. Imaging Radiat. Oncol.* 53 (2009) 248–260, <https://doi.org/10.1111/j.1754-9485.2009.02056.x>.
 - [12] M.S. Fernando, J.E. Simpson, F. Matthews, C. Brayne, C.E. Lewis, R. Barber, R. N. Kalaria, G. Forster, F. Esteves, S.B. Wharton, P.J. Shaw, J.T. O'Brien, P.G. Ince, White matter lesions in an unselected cohort of the elderly, *Stroke* 37 (2006) 1391–1398, <https://doi.org/10.1161/01.STR.0000221308.94473.14>.
 - [13] B. Fischl, D.H. Salat, E. Busa, M. Albert, M. Dieterich, C. Haselgrove, A. van der Kouwe, R. Killiany, D. Kennedy, S. Klaveness, A. Montillo, N. Makris, B. Rosen, A. M. Dale, Whole brain segmentation, *Neuron* 33 (2002) 341–355, [https://doi.org/10.1016/S0896-6273\(02\)00569-X](https://doi.org/10.1016/S0896-6273(02)00569-X).
 - [14] B. Fischl, D.H. Salat, A.J.W. van der Kouwe, N. Makris, F. Ségonne, B.T. Quinn, A. M. Dale, Sequence-independent segmentation of magnetic resonance images, *Neuroimage* 23 (2004) S69–S84, <https://doi.org/10.1016/j.neuroimage.2004.07.016>.
 - [15] D.A. Fleischman, J. Yang, K. Arfanakis, Z. Arvanitakis, S.E. Leurgans, A.D. Turner, L.L. Barnes, D.A. Bennett, A.S. Buchman, Physical activity, motor function, and white matter hyperintensity burden in healthy older adults, *Neurology* 84 (2015) 1294–1300, <https://doi.org/10.1212/WNL.0000000000001417>.
 - [16] R.A.R. Gons, A.G.W. van Norden, K.F. de Laat, L.J.B. van Oudheusden, I.W.M. van Uden, M.P. Zwiers, D.G. Norris, F.-E. de Leeuw, Cigarette smoking is associated with reduced microstructural integrity of cerebral white matter, *Brain* 134 (2011) 2116–2124, <https://doi.org/10.1093/brain/awr145>.
 - [17] L. Griffanti, M. Jenkinson, S. Suri, E. Zsoldos, A. Mahmood, N. Filippini, C. E. Sexton, A. Topiwala, C. Allan, M. Kivimäki, A. Singh-Manoux, K.P. Ebmeier, C. E. Mackay, G. Zamboni, Classification and characterization of periventricular and deep white matter hyperintensities on MRI: A study in older adults, *Neuroimage* 170 (2018) 174–181, <https://doi.org/10.1016/j.neuroimage.2017.03.024>.
 - [18] L. Griffanti, G. Zamboni, A. Khan, L. Li, G. Bonifacio, V. Sundaresan, U.G. Schulz, W. Kuker, M. Battaglini, P.M. Rothwell, M. Jenkinson, BIANCA (Brain Intensity AbNormality Classification Algorithm): A new tool for automated segmentation of white matter hyperintensities, *Neuroimage* 141 (2016) 191–205, <https://doi.org/10.1016/j.neuroimage.2016.07.018>.
 - [19] Z.-N. Guo, X. Sun, J. Liu, H. Sun, Y. Zhao, H. Ma, B. Xu, Z. Wang, C. Li, X. Yan, H. Zhou, P. Zhang, H. Jin, Y. Yang, The impact of variational primary collaterals on cerebral autoregulation, *Front. Physiol.* 9 (2018), <https://doi.org/10.3389/fphys.2018.00759>.
 - [20] M. Habes, G. Erus, J.B. Toledo, T. Zhang, N. Bryan, L.J. Launer, Y. Rosseel, D. Janowitz, J. Doshi, S. Van der Auwera, B. von Sarnowski, K. Hegenscheid, N. Hosten, G. Homuth, H. Völzke, U. Schminke, W. Hoffmann, H.J. Grabe, C. Davatzikos, White matter hyperintensities and imaging patterns of brain ageing in the general population, *Brain* 139 (2016) 1164–1179, <https://doi.org/10.1093/brain/aww008>.
 - [21] L.B. Hindenes, A.K. Häberg, L.H. Johnsen, E.B. Mathiesen, D. Robben, T. R. Vangberg, Variations in the circle of Willis in a large population sample using 3D TOF angiography: The Tromsø study, *PLoS One* 15 (2020), e0241373, <https://doi.org/10.1371/journal.pone.0241373>.
 - [22] T. Hothorn, F. Bretz, P. Westfall, Simultaneous inference in general parametric models, *Biom. J.* 50 (2008) 346–363, <https://doi.org/10.1002/bimj.200810425>.
 - [23] J. Jiang, T. Liu, W. Zhu, R. Koncz, H. Liu, T. Lee, P.S. Sachdev, W. Wen, UBO detector – a cluster-based, fully automated pipeline for extracting white matter hyperintensities, *Neuroimage* 174 (2018) 539–549, <https://doi.org/10.1016/j.neuroimage.2018.03.050>.
 - [24] K. Kamnitsas, C. Ledig, V.F.J. Newcombe, J.P. Simpson, A.D. Kane, D.K. Menon, D. Rueckert, B. Glocker, Efficient multi-scale 3D CNN with fully connected CRF for accurate brain lesion segmentation, *Med. Image Anal.* 36 (2017) 61–78, <https://doi.org/10.1016/j.media.2016.10.004>.
 - [25] K.S. King, R.M. Peshock, H.C. Rossetti, R.W. McColl, C.R. Ayers, K.M. Hulse, S. R. Das, Effect of normal aging versus hypertension, abnormal body mass index, and diabetes mellitus on white matter hyperintensity volume, *Stroke* 45 (2014) 255–257, <https://doi.org/10.1161/STROKEAHA.113.003602>.
 - [26] M.J. Krabbe-Hartkamp, J. van der Grond, F.E. de Leeuw, J.C. de Groot, A. Algra, B. Hillen, M.M. Breteler, W.P. Mali, Circle of Willis: morphologic variation on three-dimensional time-of-flight MR angiograms, *Radiology* 207 (1998) 103–111, <https://doi.org/10.1148/radiology.207.1.9530305>.
 - [27] H.J. Kuijff, A. Casamitjana, D.L. Collins, M. Dadar, A. Georgiou, M. Ghafoorian, D. Jin, A. Khademi, J. Knight, H. Li, X. Llado, J.M. Biesbroek, M. Luna, Q. Mahmood, R. McKinley, A. Mehrtash, S. Ourselin, B.-Y. Park, H. Park, S.H. Park, S. Pezold, E. Puybareau, J. De Bresser, L. Rittner, C.H. Sudre, S. Valverde, V. Vilaplana, R. Wiest, Y. Xu, Z. Xu, G. Zeng, J. Zhang, G. Zheng, R. Heinen, C. Chen, W. van der Flier, F. Barkhof, M.A. Viergever, G.J. Biessels, S. Andermatt, M. Bento, M. Berseth, M. Belyaev, M.J. Cardoso, Standardized assessment of automatic segmentation of white matter hyperintensities and results of the WMH segmentation challenge, *IEEE Trans. Med. Imaging* 38 (2019) 2556–2568, <https://doi.org/10.1109/TMI.2019.2905770>.
 - [28] H. Li, G. Jiang, J. Zhang, R. Wang, Z. Wang, W.-S. Zheng, B. Menze, Fully convolutional network ensembles for white matter hyperintensities segmentation in MR images, *Neuroimage* 183 (2018) 650–665, <https://doi.org/10.1016/j.neuroimage.2018.07.005>.
 - [29] H. Li, Y. Xiong, G. Xu, R. Zhang, W. Zhu, Q. Yin, M. Ma, X. Fan, F. Yang, W. Liu, Z. Duan, X. Liu, The circle of Willis and White matter lesions in patients with carotid atherosclerosis, *J. Stroke Cerebrovasc. Dis.* 24 (2015) 1749–1754, <https://doi.org/10.1016/j.jstrokecerebrovasdis.2015.03.048>.
 - [30] I. Njølstad, E.B. Mathiesen, H. Schirmer, D.S. Thelle, The Tromsø study 1974–2016: 40 years of cardiovascular research, *Scand. Cardiovasc. J.* 50 (2016) 276–281, <https://doi.org/10.1080/14017431.2016.1239837>.
 - [31] P.A. Nyquist, M. Bilgel, R. Gottesman, L.R. Yanek, T.F. Moy, L.C. Becker, J. L. Cuzzocreo, J. Prince, B.A. Wasserman, D.M. Yousem, D.M. Becker, B.G. Kral, D. Vaidya, Age differences in periventricular and deep white matter lesions, *Neurobiol. Aging* 36 (2015) 1653–1658, <https://doi.org/10.1016/j.neurobiolaging.2015.01.005>.
 - [32] R. Pascual, V.A. Padurean, D. Bartoš, A. Bartoš, B.A. Szabo, The geometry of the circle of Willis anatomical variants as a potential cerebrovascular risk factor, *Turk. Neurosurg.* (2018), <https://doi.org/10.5137/1019-5149.JTN.21835-17.3>.
 - [33] S. Purkayastha, O. Fadar, A. Mehregan, D.H. Salat, N. Moscufo, D.S. Meier, C. R. Guttmann, N.D. Fisher, L.A. Lipsitz, F.A. Sorond, Impaired cerebrovascular hemodynamics are associated with cerebral white matter damage, *J. Cereb. Blood Flow Metab.* 34 (2014) 228–234, <https://doi.org/10.1038/jcbfm.2013.180>.
 - [34] C. Qiu, Y. Zhang, C. Xue, S. Jiang, W. Zhang, MRA study on variation of the circle of Willis in healthy Chinese male adults, *Biomed. Res. Int.* 2015 (2015) 8, <https://doi.org/10.1155/2015/976340>.
 - [35] M.F. Rachmadi, M.C. del Valdés-Hernández, M.L.F. Agan, C. Di Perri, T. Komura, Segmentation of white matter hyperintensities using convolutional neural networks with global spatial information in routine clinical brain MRI with none or mild vascular pathology, *Comput. Med. Imaging Graph.* 66 (2018) 28–43, <https://doi.org/10.1016/j.compmedimag.2018.02.002>.
 - [36] E. Rostrup, A.A. Gouw, H. Vrenken, E.C.W. van Straaten, S. Ropele, L. Pantoni, D. Inzitari, F. Barkhof, G. Waldemar, The spatial distribution of age-related white matter changes as a function of vascular risk factors—results from the LADIS study, *Neuroimage* 60 (2012) 1597–1607, <https://doi.org/10.1016/j.neuroimage.2012.01.106>.
 - [37] D.J. Ryan, S. Byrne, R. Dunne, M. Harmon, J. Harbison, White matter disease and an incomplete circle of Willis, *Int. J. Stroke* 10 (2015) 547–552, <https://doi.org/10.1111/ijis.12042>.
 - [38] L. Saba, E. Raz, G. Fatterpekar, R. Montisci, M. di Martino, P.P. Bassareo, M. Piga, Correlation between leukoaraiosis volume and circle of Willis variants, *J. Neuroimaging* 25 (2015) 226–231, <https://doi.org/10.1111/jon.12103>.
 - [39] L. Saba, R. Sanfilippo, M. Porcu, P. Lucatelli, R. Montisci, F. Zaccagna, J.S. Suri, M. Anzidei, M. Wintermark, Relationship between white matter hyperintensities volume and the circle of Willis configurations in patients with carotid artery pathology, *Eur. J. Radiol.* 89 (2017) 111–116, <https://doi.org/10.1016/j.ejrad.2017.01.031>.
 - [40] C.L. Satizabal, Y.C. Zhu, B. Mazoyer, C. Dufouil, C. Tzourio, Circulating IL-6 and CRP are associated with MRI findings in the elderly: the 3C-Dijon study, *Neurology* 78 (2012) 720–727, <https://doi.org/10.1212/WNL.0b013e318248e50f>.
 - [41] P. Schmidt, C. Gaser, M. Arsic, D. Buck, A. Förschler, A. Berthele, M. Hoshi, R. Ilg, V.J. Schmid, C. Zimmer, B. Hemmer, M. Mühlau, An automated tool for detection of FLAIR-hyperintense white-matter lesions in multiple sclerosis, *Neuroimage* 59 (2012) 3774–3783, <https://doi.org/10.1016/j.neuroimage.2011.11.032>.
 - [42] N. Takaya, C. Yuan, B. Chu, T. Saam, N.L. Polissar, G.P. Jarvik, C. Isaac, J. McDonough, C. Natiello, R. Small, M.S. Ferguson, T.S. Hatsukami, Presence of intraplate hemorrhage stimulates progression of carotid atherosclerotic plaques, *Circulation* 111 (2005) 2768–2775, <https://doi.org/10.1161/CIRCULATIONAHA.104.504167>.
 - [43] V.H. ten Dam, D.M.J. van den Heuvel, A.J.M. de Craen, E.L.E.M. Bollen, H. M. Murray, R.G.J. Westendorp, G.J. Blauw, M.A. van Buchem, Decline in total cerebral blood flow is linked with increase in periventricular but not deep white matter hyperintensities, *Radiology* 243 (2007) 198–203, <https://doi.org/10.1148/radiol.2431052111>.
 - [44] S. Valverde, M. Cabezas, E. Roura, S. González-Villà, D. Pareto, J.C. Vilanova, L. Ramió-Torrentà, A. Rovira, A. Oliver, X. Lladó, Improving automated multiple sclerosis lesion segmentation with a cascaded 3D convolutional neural network approach, *Neuroimage* 155 (2017) 159–168, <https://doi.org/10.1016/j.neuroimage.2017.04.034>.
 - [45] J. van der Grond, A.F. van Raamt, Y. van der Graaf, W.P.T.M. Mali, R.H. C. Bisschops, A fetal circle of Willis is associated with a decreased deep white matter lesion load, *Neurology* 63 (2004) 1452–1456, <https://doi.org/10.1212/01.WNL.0000142041.42491.F4>.
 - [46] E.J. van Dijk, M.M.B. Breteler, R. Schmidt, K. Berger, L.-G. Nilsson, M. Oudkerk, A. Pajak, S. Sans, M. de Ridder, C. Dufouil, R. Fuhrer, S. Giampaoli, L.J. Launer, A. Hofman, The association between blood pressure, hypertension, and cerebral white matter lesions: cardiovascular determinants of dementia study, *Hypertension* 44 (2004) 625–630, <https://doi.org/10.1161/01.HYP.0000145857.98904.20>.
 - [47] E.J. van Dijk, N.D. Prins, H.A. Vrooman, A. Hofman, P.J. Koudstaal, M.M. B. Breteler, Progression of cerebral small vessel disease in relation to risk factors and cognitive consequences, *Stroke* 39 (2008) 2712–2719, <https://doi.org/10.1161/STROKEAHA.107.513176>.
 - [48] P.J. van Laar, J. Hendrikse, X. Golay, H. Lu, M.J.P. Van Osch, J. Van Der Grond, In vivo flow territory mapping of major brain feeding arteries, *Neuroimage* 29 (2006) 136–144, <https://doi.org/10.1016/j.neuroimage.2005.07.011>.
 - [49] E.C.W. van Straaten, F. Fazekas, E. Rostrup, P. Scheltens, R. Schmidt, L. Pantoni, D. Inzitari, G. Waldemar, T. Erkinjuntti, R. Mäntylä, L.-O. Wahlund, F. Barkhof, Impact of white matter hyperintensities scoring method on correlations with clinical data, *Stroke* 37 (2006) 836–840, <https://doi.org/10.1161/01.STR.0000202585.26325.74>.
 - [50] Z. Vrselja, H. Brkic, S. Mrdenovic, R. Radic, G. Curic, Function of circle of Willis, *J. Cereb. Blood Flow Metab.* 34 (2014) 578–584, <https://doi.org/10.1038/jcbfm.2014.7>.

- [51] J.M. Wardlaw, M.C. Valdés Hernández, S. Muñoz-Maniega, What are white matter hyperintensities made of? Relevance to vascular cognitive impairment, *J. Am. Heart Assoc.* 4 (2015), e001140, <https://doi.org/10.1161/JAHA.114.001140>.
- [52] P. Wijesinghe, H.W.M. Steinbusch, S.K. Shankar, T.C. Yasha, K.R.D. De Silva, Circle of Willis abnormalities and their clinical importance in ageing brains: a cadaveric anatomical and pathological study, *J. Chem. Neuroanat.* 106 (2020) 101772, <https://doi.org/10.1016/j.jchemneu.2020.101772>.
- [53] G. Xu, B. Liu, Y. Sun, Y. Du, L.G. Snetselaar, F.B. Hu, W. Bao, Prevalence of diagnosed type 1 and type 2 diabetes among US adults in 2016 and 2017: population based study, *BMJ* (2018), <https://doi.org/10.1136/bmj.k1497> k1497.
- [54] H. Ye, X. Wu, J. Yan, J. Wang, J. Qiu, Y. Wang, Completeness of circle of Willis and white matter hyperintensities in patients with severe internal carotid artery stenosis, *Neurol. Sci.* 40 (2019) 509–514, <https://doi.org/10.1007/s10072-018-3683-9>.
- [55] O.A. Zaninovich, W.L. Ramey, C.M. Walter, T.M. Dumont, Completion of the circle of Willis varies by gender, age, and indication for computed tomography angiography, *World Neurosurg.* 106 (2017) 953–963, <https://doi.org/10.1016/j.wneu.2017.07.084>.
- [56] C. Zhou, C. Yuan, R. Li, W. Wang, C. Li, X. Zhao, Association between incomplete circle of Willis and carotid vulnerable atherosclerotic plaques, *Arterioscler. Thromb. Vasc. Biol.* 38 (2018) 2744–2749, <https://doi.org/10.1161/ATVBAHA.118.311797>.